

# A Study of Avalon<sup>K2</sup>

# Avalon<sup>K2</sup>



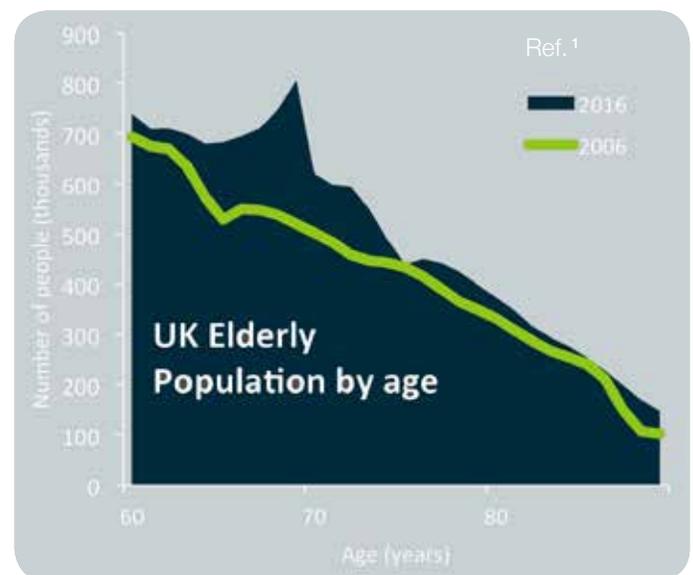
Hydraulic prosthetic feet can improve mobility and independence for limited community ambulators.

The main driving force behind advancing lower limb prosthetic technology in the 21st century is biomimetic design; reproducing the biomechanical performance of natural limbs. Inherent in this is recognising that different demographics of the amputee population have different biomechanical requirements, and that the engineering principles behind different devices must accommodate for this.

## Amputee Demographics

The global trends of increasing ageing population and incidence of chronic disease in developed countries are well known. Over 60s make up approximately 23% of the UK population – approximately 14.7 million people<sup>1</sup>. The Office for National Statistics reports that this proportion has grown by 21% in the last 10 years<sup>1</sup>. This trend is consistent with that in the United States where over 60s make up approximately 20.3% of the population – 65.5 million people<sup>2</sup>. Globally, almost 1 in 10 people are over 60 and by 2050, this is estimated to become 1 in 5 people<sup>3</sup>.

The prevalence of diabetes and cardiovascular disease increases with age<sup>4</sup>, with vascular disease being the cause of over 80% of lower limb amputations<sup>5,6</sup>. There are 5200 lower limb amputations per year in the UK<sup>5</sup> and 185,000 in the US<sup>7</sup>, of which 75% occur in over 60s<sup>5,6</sup>.



## The Biomechanics of Elderly Gait

It is well documented that there are a number of biomechanical differences between the gait of elderly people and that of young people<sup>8</sup>. Older people tend to walk more slowly<sup>9,10</sup>, contributing to a shorter step and stride length<sup>9-11</sup>. These differences affect the ranges of motion of the joints, predominantly through plantarflexion of the ankle and extension of the hip<sup>9-12</sup>. Lower limb muscle weakness is common amongst elderly people and therefore the power generated by the ankle in late stance is significantly reduced<sup>11,13</sup>.

**10%**  
Reduction  
in walking speed<sup>10</sup>

**11%**  
Shorter  
stride length<sup>10</sup>

**17%**  
Less ankle  
power generated  
in late stance<sup>11</sup>

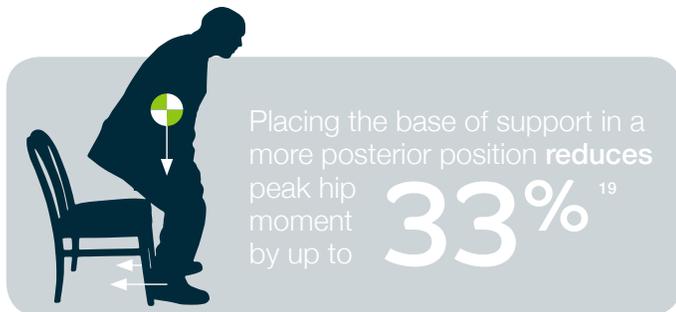
All of these differences influence the motion of the body's centre-of-mass in relation to its base of support at the ground, and must be considered during prosthetic foot design. Elderly amputees

are often described as being ‘Activity Level 2’ which refers to someone who has the “ability or potential for ambulation with the ability to traverse low-level environmental barriers such as curbs, stairs, or uneven surfaces”. Older people also have a much greater variability in their gait<sup>10,14–16</sup> meaning a prosthesis that can provide consistency and predictability of function is of even greater importance in order to ensure safety.

## Domestic Independence

Older people tend to spend less time outside and more time around the home. This means for those with lower mobility capabilities, functional domestic tasks, such as rising from a chair, become imperative to maintaining independence and quality of life. In fact, the transition from a seated position to standing has been described as “the most mechanically demanding functional task routinely undertaken during daily activities”<sup>17</sup>.

Older people can adapt their movement strategy to account for their abilities. When rising from a chair, if they bring their feet to a more posterior position they reduce the distance between their body’s centre-of-mass and their base of support<sup>18</sup>. Consequently, there is less demand on the lower limb muscles and joints, allowing them to generate enough force to stand more easily<sup>19–21</sup>. Scientific studies have identified foot placement as a critical factor in the sit-to-stand movement<sup>22</sup>. Consideration of foot placement and the ankle range of motion in prosthetic design enables a more optimised body posture and movement that requires less effort.



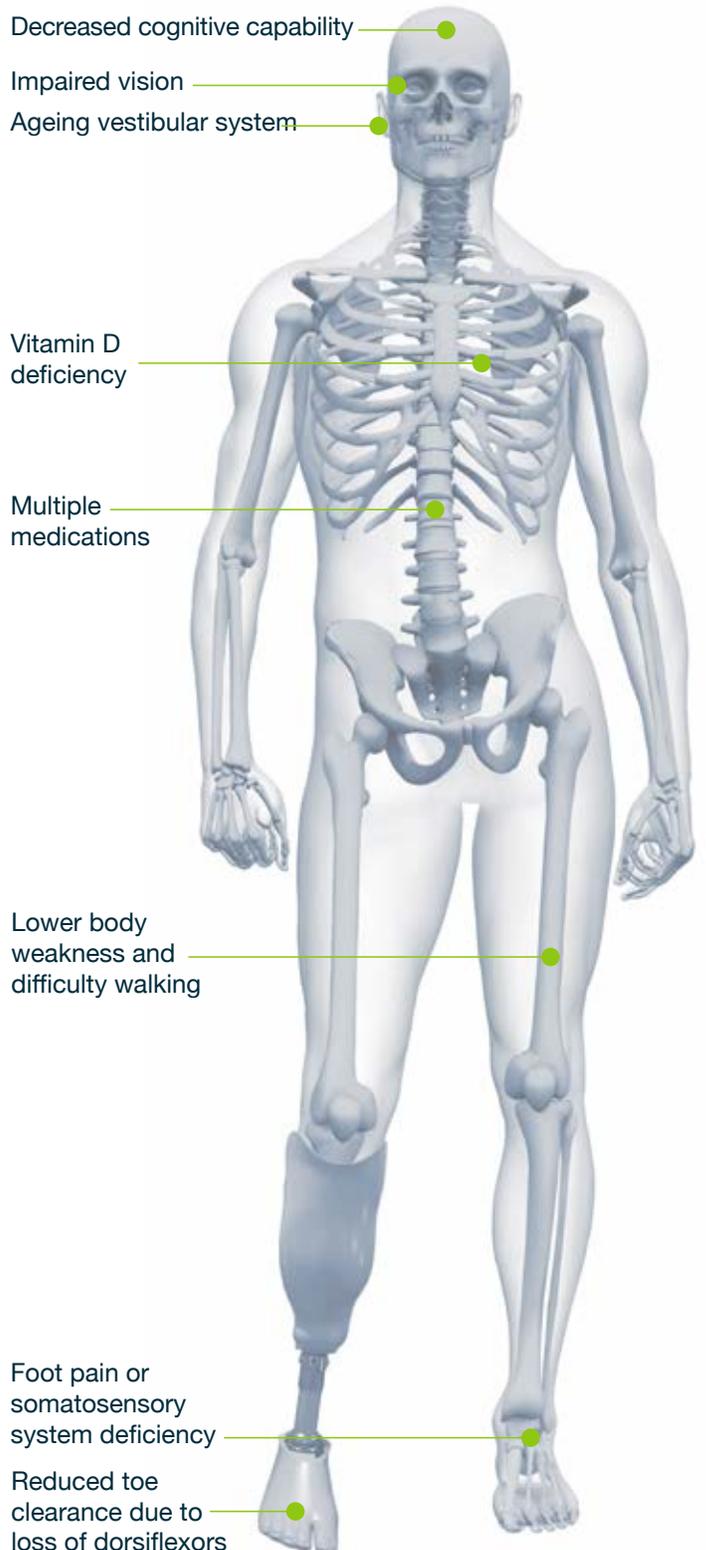
## The Risk of Falling

Gait patterns are a significant contributor to the risk of falling in the elderly<sup>23,24</sup>. Their increased variability from one step to the next has been linked to the frequency of falling<sup>10,25–28</sup>, as has shorter stride length, reduced plantarflexion and reduced hip extension<sup>27</sup>.

Other common characteristics of advanced age make elderly people more susceptible to the risk of falls<sup>29</sup>. As vision deteriorates, there is a greater reliance on other sensory inputs to detect potential trip hazards, and as the central nervous system ages, a decline in cognitive ability can occur. The vestibular system, which provides sensory information regarding motion, spatial awareness and balance, begins to weaken and becomes less reliable. Poor circulation leads to peripheral neuropathy, reducing sensation at the extremities, slowing reactions to external stimuli, such as changes in slope or uneven terrain.

Beyond physical characteristics, certain medications, such as those for high blood pressure or painkillers, have shown a correlation with the likelihood of falling. Particularly at risk are those who are taking multiple medications at once<sup>30,31</sup>.

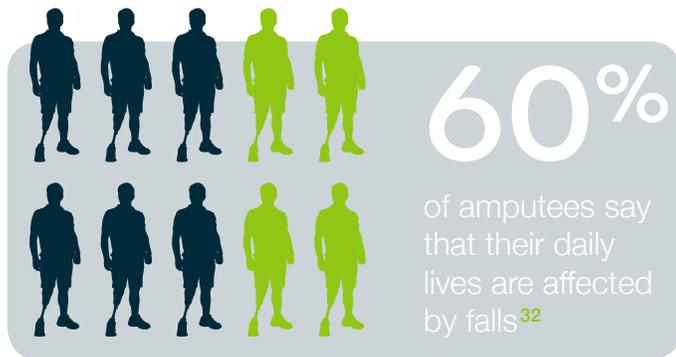
Studies looking at amputee falls indicate 58% of unilateral amputees fall at least once a year<sup>32</sup>. Of those who fell, 50% sustained a tissue injury, while 7% required hospital treatment<sup>32</sup>. Other effects of falls include broken bones, head injuries<sup>33,34</sup> and a loss of independence<sup>31,35,36</sup>, that can severely affect the quality of life of the amputee.



## The Cost of Falls

As well as physical consequences, falls can impact other areas of life. 60% of amputees who fall say it affects their daily life and 36% report a loss of confidence<sup>32</sup>.

Falls can also cause a financial burden, both on the amputee and their family if extra social care is required, and to the economy as a whole. In 2000, in the United States, medical costs for falls totalled \$19.2 billion<sup>37</sup>. Reducing the risk of falls and the need for institutional care has the potential for a positive health-economic effect due to reduced care cost over time.



## Vascular Health

The majority of elderly amputees have an amputation aetiology relating to vascular disease or diabetes<sup>5</sup>. The resulting poor circulation and impaired sensation mean the skin and soft tissue of the residuum are vulnerable to irritation and damage. Any resulting wounds heal more slowly and are vulnerable to infection. An infected wound may potentially necessitate further amputation surgery.

## Musculoskeletal Concerns

Amputees walk with more reliance on the unaffected leg and asymmetry of gait and standing has been linked to the increased likelihood of developing osteoarthritis<sup>38-40</sup> which is two to three times higher among amputees<sup>38</sup>, and an increased chance of developing back pain<sup>41</sup>. In fact, 60% of amputees report moderate to extreme back pain within two years of amputation<sup>42</sup>.

## Advanced Technology Can Advance Functional Ability

It is common for health services to prescribe inexpensive devices with restricted function to limited community walkers. Prosthetic interventions that are specifically designed for the biomechanical requirements of the older user could help reduce the risk of falls, maintain greater mobility and independence, improve quality of life and help reduce the long term burden on health care services.

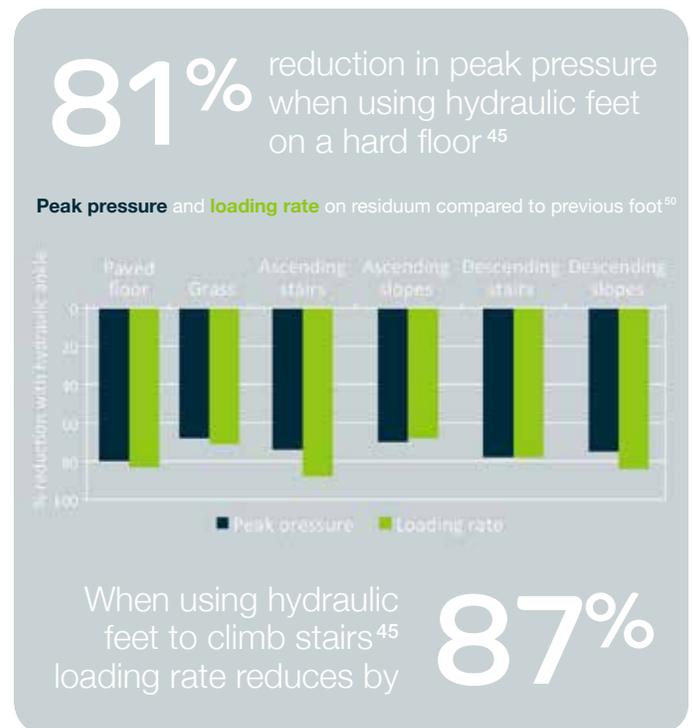
## Hydraulic Ankle Technology

Conventional prostheses are usually firmly attached to the shin or 'pylon' and rely on the deflection or deformation of polymeric foot components to replicate the dorsiflexion and plantarflexion behaviour of the natural ankle. Models of the biological foot have shown that this elastic behaviour is present at normal walking speeds<sup>43</sup>. However, at slow

speeds, the ankle becomes a net absorber of energy and the elastic model no longer fits<sup>43</sup>. The viscoelastic behaviour of hydraulic ankles better replicates natural ankle biomechanics.

Hydraulic ankle technology has been proven to provide a number of benefits to elderly amputees. During walking, the deformable components of a prosthesis are deflected when loaded and return to their original position when unloaded. With a hydraulic ankle, when unloaded, the ankle joint remains in a dorsiflexed position, meaning that the toe clearance during swing phase is increased by 18%<sup>44</sup> so there is less chance of catching the foot on the ground or another object and a trip occurring.

The damped motion of the ankle joint also absorbs energy and reduces the loading on the residual limb within the socket. One study measured reductions in peak pressures by up to 81% and in the rate of loading by up to 87%, during a number of different everyday activities<sup>45</sup>. Hydraulic prosthetic ankles seek to mimic biological ankle action with a hydraulically-damped, articulating joint in combination with the deformable foot.



## The Avalon<sup>K2</sup> Effect

Avalon<sup>K2</sup> was designed specifically to cater for the biomechanical requirements of older or less active, Activity Level 2 users. It enhances walking confidence because it hydraulically adjusts to inclines and steps. The hydraulic dorsiflexion movement also enhances comfort and balance when sitting down, standing up from a chair or crouching down. Avalon<sup>K2</sup> self-aligns to secure the knee joint and encourage good posture and joint position, this enhances transfemoral knee stability to help prevent falls and it reduces unwanted moments on the knee joint of transtibial users. The ankle dorsiflexes after mid stance and 'toes' remain elevated during swing phase leading to increased ground clearance for safety and efficiency, providing the best performance for Activity Level 2 biomechanics.

## Clinical Evidence for Avalon<sup>K2</sup>

### Improved Symmetry

One study sought to measure the impact of Avalon<sup>K2</sup> compared to non-hydraulic designs, with regards to Activity Level 2 amputees<sup>50</sup>.

A mixed group comprising unilateral and bilateral, above and below knee amputees participated in the study. Their gait was assessed with their habitual foot whilst walking at a self-selected speed. Afterwards, these same amputees were provided with Avalon<sup>K2</sup> hydraulic feet and given four weeks to acclimatise. After the acclimatisation period, their gait was assessed again.

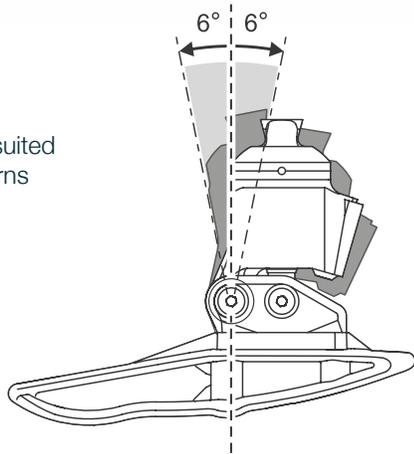
The result of this study was measured by the time for which weight was borne on each leg, with a particular focus on asymmetry between their limbs. Typically, amongst amputees, stance phase duration is longer on the sound side because their residuum may be painful to load, they may have a lack of prosthesis control or there may be a lack of stability provided by the prosthesis. This asymmetry has detrimental consequences for stability and long term health.

Three quarters of the amputees saw a reduction in asymmetry between the two limbs giving a mean reduction of 34%. The greatest improvement observed was for a unilateral below knee amputee, who saw an 86% reduction in asymmetry. When weight bearing is more evenly distributed, there are improvements in gait stability and postural sway. These factors act to reduce the risk of falling, as well as the risk of developing back pain. When there is less reliance on the sound limb for weight bearing, the chances of long term health problems such as osteoarthritis in the joints or lower back pain are reduced.

Hydraulic ankle technology controls plantar and dorsiflexion

Ergonomic keel achieves a comfortable rollover action

Ankle range of motion suited to elderly walking patterns



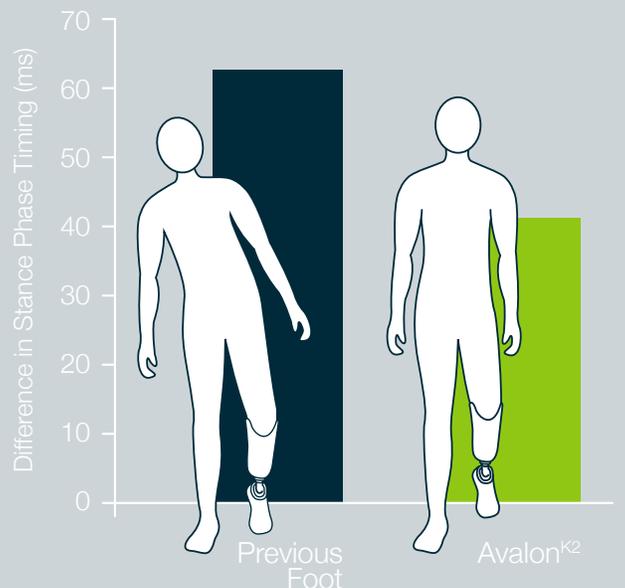
### Features:

- Waterproof K2 hydraulic ankle foot
- Optimised keel for ease of rollover
- Single valve adjustment for simultaneous plantarflexion and dorsiflexion
- Plantarflexion compliance when descending slopes
- Sandal toe allows different footwear styles

The most energy efficient “rollover” shape has been identified as 30% of the walker’s leg length<sup>46,47</sup>. Evidence suggests that when walking at different speeds and on changing inclines, people will adapt other gait kinematics in order to maintain this consistent rollover shape<sup>48</sup>. For a person of a typical adult height between 1.5m and 1.8m, this equates to approximately 245-290mm. The geometry for the Avalon<sup>K2</sup> keel has been measured to produce a rollover shape of ~250mm<sup>49</sup> of which this rollover is consistent, regardless of footwear<sup>49</sup>.

Another design consideration of Avalon<sup>K2</sup> was the action of standing from a chair. The keel and shape, along with the 6° of dorsiflexion permitted by the hydraulic ankle, help move the base of support closer to the body’s centre-of-mass. Having the feet in a more posterior position reduces joint moments<sup>18-21</sup>, making it easier for the user to perform the movement.

**34%** reduction in asymmetry when using Avalon<sup>K2</sup>, compared to a non-hydraulic foot<sup>50</sup>



## User Satisfaction

21.9% increase in gait satisfaction with Avalon<sup>K2</sup> 51

Patient feedback ratings when using previous foot and Avalon<sup>K2</sup> 51



In another investigation<sup>51</sup>, 14 Activity Level 2 users, originally Multiflex wearers were surveyed using the Seattle Prosthesis Evaluation Questionnaire (PEQ) for both Multiflex and Avalon<sup>K2</sup>. The group consisted of 12 below knee amputees including one bilateral, and two above knee amputees. The group evaluated their Multiflex feet at the start of the research programme, they then wore Avalon<sup>K2</sup> for a period of four weeks, before completing the same Questionnaire. This scientifically validated instrument asks the amputee about all aspects of their prosthesis through six distinct subsets of questions from mobility capabilities and utility to hygiene and well being.

When evaluating the results, the mean scores throughout the six question categories were consistently higher for Avalon<sup>K2</sup>. The mean improvement across all categories was 14.7% and included a 17.3% improvement in ambulation, a 17.2% improvement in prosthesis satisfaction and a 21.9% increase in gait satisfaction. When broken down by amputation level, transtibial amputees had a mean improvement across all categories of 16.6%. For transfemoral amputees the cross-category mean improvement was 6.2%.

Amputees' perceptions of their own abilities are an important element in prosthetic design. In a published survey<sup>52</sup>, a mixture of Activity Level 2 and 3 amputees rated their self-assessed



abilities with hydraulic feet, compared to their prescribed feet. They were asked to rate their ability sitting and standing from chairs of different heights, getting in and out of cars and using the bathroom. Bilateral amputees particularly benefitted from the hydraulic feet, with the average score out of 100 increasing by approximately 12 points. This emphasises the suitability of the Avalon<sup>K2</sup> design for Activity Level 2 amputees, providing the necessary performance for activities of daily life and maintaining independence.

### Increased Walking Speed

For lower mobility amputees, the distance they are able to walk in two minutes is a simple clinical test to indicate the outcome of a prosthetic intervention. One group of researchers performed such tests with five unilateral below knee amputees<sup>53</sup>. Each performed the tests wearing a Navigator foot and an Avalon<sup>K2</sup>. Navigator uses the same keel design and shape as Avalon<sup>K2</sup>, but doesn't have an articulating, hydraulic ankle component, so observed differences could be attributed to this additional component. As part of the same study, biomechanical measures were investigated using 3D gait analysis.

All amputees taking part walked further with Avalon<sup>K2</sup> with

a mean walking speed increase of 6.5%. From the gait analysis, it was discovered that participants displayed more symmetrical inter-limb loading – which is related to reducing the risk of back and joint pain development – and a smoother progression of the centre-of-pressure during gait.



## Conclusion

The clinical needs of patients must drive prosthetic design. The engineering principles of the design and the technical specifications of its performance must cater to the targeted demographic of amputees.

For limited community ambulators, a change in practice for the prescription of prosthetic feet could provide improved long term outcomes. More advanced technology such as Avalon<sup>K2</sup>, a hydraulic foot specifically designed to cater for the older user's requirements, could not only be beneficial for the safety and health of the user, but could also be a more sound investment in terms of healthcare economics, helping to reduce the costs associated with fall related injuries and tissue health complaints.

# References

- Office for National Statistics (ONS). Population Estimates for UK, England and Wales, Scotland and Northern Ireland: mid-2016.2017.
- Aging Statistics [Internet]. [cited 2016 Sep 27]. Available from: [http://www.aoa.acl.gov/Aging\\_Statistics/index.aspx](http://www.aoa.acl.gov/Aging_Statistics/index.aspx)
- Global ageing statistics | Data on ageing | HelpAge International [Internet]. [cited 2016 Sep 27]. Available from: <http://www.helpage.org/resources/ageing-data/global-ageing-statistics/>
- Halter JB, Musi N, Horne FM, Crandall JP, Goldberg A, Harkless L, et al. Diabetes and cardiovascular disease in older adults: current status and future directions. *Diabetes*. 2014;63(8):2578–2589.
- Scottish Physiotherapy Amputee Research Group (SPARG). A Survey of the Lower Limb Amputee Population in Scotland. 2010.
- Fletcher DD, Andrews KL, Butters MA, Jacobsen SJ, Rowland CM, Hallett JW. Rehabilitation of the geriatric vascular amputee patient: a population-based study. *Arch Phys Med Rehabil*. 2001;82(6):776–779.
- Ziegler-Graham K, MacKenzie EJ, Ephraim PL, Trivison TG, Brookmeyer R. Estimating the prevalence of limb loss in the United States: 2005 to 2050. *Arch Phys Med Rehabil*. 2008;89(3):422–429.
- Prince F, Corriveau H, Hébert R, Winter DA. Gait in the elderly. *Gait Posture*. 1997;5(2):128–135.
- Hageman PA, Blanke DJ. Comparison of gait of young women and elderly women. *Phys Ther*. 1986;66(9):1382–1387.
- Kerrigan DC, Lee LW, Collins JJ, Riley PO, Lipsitz LA. Reduced hip extension during walking: healthy elderly and fallers versus young adults. *Arch Phys Med Rehabil*. 2001;82(1):26–30.
- Judge JO, Davis RB, Öunpuu S. Step length reductions in advanced age: the role of ankle and hip kinetics. *J Gerontol A Biol Sci Med Sci*. 1996;51(6):M303–M312.
- Kerrigan DC, Todd MK, Della Croce U, Lipsitz LA, Collins JJ. Biomechanical gait alterations independent of speed in the healthy elderly: evidence for specific limiting impairments. *Arch Phys Med Rehabil*. 1998;79(3):317–322.
- Kerrigan DC, Lee LW, Nieto TJ, Markman JD, Collins JJ, Riley PO. Kinetic alterations independent of walking speed in elderly fallers. *Arch Phys Med Rehabil*. 2000;81(6):730–735.
- Owings TM, Grabiner MD. Variability of step kinematics in young and older adults. *Gait Posture*. 2004;20(1):26–29.
- Brach JS, Studenski S, Perera S, VanSwearingen JM, Newman AB. Stance time and step width variability have unique contributing impairments in older persons. *Gait Posture*. 2008;27(3):431–439.
- Mills PM, Barrett RS. Swing phase mechanics of healthy young and elderly men. *Hum Mov Sci*. 2001;20(4):427–446.
- Riley PO, Schenkman ML, Mann RW, Hodge WA. Mechanics of a constrained chair-rise. *J Biomech*. 1991;24(1):77–85.
- Papa E, Cappozzo A. Sit-to-stand motor strategies investigated in able-bodied young and elderly subjects. *J Biomech*. 2000;33(9):1113–1122.
- Shepherd RB, Koh HP. Some biomechanical consequences of varying foot placement in sit-to-stand in young women. *Scand J Rehabil Med*. 1996;28(2):79–88.
- Janssen WG, Bussmann HB, Stam HJ. Determinants of the sit-to-stand movement: a review. *Phys Ther*. 2002;82(9):866–879.
- Bernardi M, Rosponi A, Castellano V, Rodio A, Traballesi M, Delussi AS, et al. Determinants of sit-to-stand capability in the motor impaired elderly. *J Electromyogr Kinesiol*. 2004;14(3):401–410.
- Kawagoe S, Tajima N, Chosa E. Biomechanical analysis of effects of foot placement with varying chair height on the motion of standing up. *J Orthop Sci Off J Jpn Orthop Assoc*. 2000;5(2):124–33.
- WISQARS (Web-based Injury Statistics Query and Reporting System)[Injury Center]CDC [Internet]. [cited 2016 Aug 18]. Available from: <https://www.cdc.gov/injury/wisqars/>
- Miller WC, Speechley M, Deathe B. The prevalence and risk factors of falling and fear of falling among lower extremity amputees. *Arch Phys Med Rehabil*. 2001;82(8):1031–1037.
- Hausdorff JM, Edelberg HK, Mitchell SL, Goldberger AL, Wei JY. Increased gait unsteadiness in community-dwelling elderly fallers. *Arch Phys Med Rehabil*. 1997;78(3):278–283.
- Hausdorff JM, Rios DA, Edelberg HK. Gait variability and fall risk in community-living older adults: a 1-year prospective study. *Arch Phys Med Rehabil*. 2001;82(8):1050–1056.
- Barak Y, Wagenaar RC, Holt KG. Gait characteristics of elderly people with a history of falls: a dynamic approach. *Phys Ther*. 2006;86(11):1501–1510.
- Barrett RS, Mills PM, Begg RK. A systematic review of the effect of ageing and falls history on minimum foot clearance characteristics during level walking. *Gait Posture*. 2010;32(4):429–435.
- Tromp AM, Pluijm SMF, Smit JH, Deeg DJH, Bouter LM, Lips P. Fall-risk screening test: a prospective study on predictors for falls in community-dwelling elderly. *J Clin Epidemiol*. 2001;54(8):837–844.
- Important Facts about Falls | Home and Recreational Safety | CDC Injury Center [Internet]. [cited 2016 Aug 18]. Available from: <http://www.cdc.gov/homeandrecreationsafety/falls/adultfalls.html>
- Hunter SW, Batchelor F, Hill KD, Hill A-M, Mackintosh S, Payne M. Risk factors for falls in people with a lower limb amputation: a systematic review. *PM&R*. 2016
- Kulkarni J, Wright S, Toole C, Morris J, Hiron R. Falls in patients with lower limb amputations: prevalence and contributing factors. *Physiotherapy*. 1996;82(2):130–136.
- Alexander BH, Rivara FP, Wolf ME. The cost and frequency of hospitalization for fall-related injuries in older adults. *Am J Public Health*. 1992;82(7):1020–1023.
- Sterling DA, O'Connor JA, Bonadies J. Geriatric falls: injury severity is high and disproportionate to mechanism. *J Trauma Acute Care Surg*. 2001;50(1):116–119.
- Miller WC, Deathe AB. The influence of balance confidence on social activity after discharge from prosthetic rehabilitation for first lower limb amputation. *Prosthet Orthot Int*. 2011;35(4):379–385.
- Costs of Falls Among Older Adults | Home and Recreational Safety | CDC Injury Center [Internet]. [cited 2016 Aug 18]. Available from: <http://www.cdc.gov/homeandrecreationsafety/falls/fallcost.html>
- Stevens JA, Corso PS, Finkelstein EA, Miller TR. The costs of fatal and non-fatal falls among older adults. *Inj Prev*. 2006;12(5):290–295.
- Burke MJ, Roman V, Wright V. Bone and joint changes in lower limb amputees. *Ann Rheum Dis*. 1978;37(3):252–254.
- Kulkarni J, Adams J, Thomas E, Silman A. Association between amputation, arthritis and osteopenia in British male war veterans with major lower limb amputations. *Clin Rehabil*. 1998;12(4):348–353.
- Norvell DC, Czerniecki JM, Reiber GE, Maynard C, Pecoraro JA, Weiss NS. The prevalence of knee pain and symptomatic knee osteoarthritis among veteran traumatic amputees and nonamputees. *Arch Phys Med Rehabil*. 2005;86(3):487–493.
- Ehde DM, Czerniecki JM, Smith DG, Campbell KM, Edwards WT, Jensen MP, et al. Chronic phantom sensations, phantom pain, residual limb pain, and other regional pain after lower limb amputation. *Arch Phys Med Rehabil*. 2000;81(8):1039–1044.
- Kulkarni J, Gaine WJ, Buckley JG, Rankine JJ, Adams J. Chronic low back pain in traumatic lower limb amputees. *Clin Rehabil*. 2005;19(1):81–86.
- Hansen AH, Childress DS, Miff SC, Gard SA, Mesplay KP. The human ankle during walking: implications for design of biomimetic ankle prostheses. *J Biomech*. 2004;37(10):1467–1474.
- Johnson L, De Asha AR, Munjal R, Kulkarni J, Buckley JG. Toe clearance when walking in people with unilateral transtibial amputation: effects of passive hydraulic ankle. *J Rehabil Res Dev*. 2014;51(3):429.
- Portnoy S, Kristal A, Gefen A, Siev-Ner I. Outdoor dynamic subject-specific evaluation of internal stresses in the residual limb: hydraulic energy-stored prosthetic foot compared to conventional energy-stored prosthetic feet. *Gait Posture*. 2012;35(1):121–125.
- Adamczyk PG, Collins SH, Kuo AD. The advantages of a rolling foot in human walking. *J Exp Biol*. 2006;209(20):3953–3963.
- Hansen AH, Wang CC. Effective rocker shapes used by able-bodied persons for walking and fore-aft swaying: Implications for design of ankle-foot prostheses. *Gait Posture*. 2010;32(2):181–184.
- Hansen AH, Childress DS. Investigations of roll-over shape: Implications for design, alignment, and evaluation of ankle-foot prostheses and orthoses. *Disabil Rehabil*. 2010;32(26):2201–2209.
- Curtze C, Hof AL, van Keeken HG, Halbertsma JP, Postema K, Otten B. Comparative roll-over analysis of prosthetic feet. *J Biomech*. 2009;42(11):1746–1753.
- Moore R. Effect on Stance Phase Timing Asymmetry in Individuals with Amputation Using Hydraulic Ankle Units. *JPO J Prosthet Orthot*. 2016;28(1):44–48.
- Moore R. Patient evaluation of a novel prosthetic foot with hydraulic ankle aimed at persons with amputation with lower activity levels. *JPO: Journal of Prosthetics and Orthotics*. 2017;29(1):44–7.
- Sedki I, Moore R. Patient evaluation of the Echelon foot using the Seattle Prosthesis Evaluation Questionnaire. *Prosthet Orthot Int*. 2013;37(3):250–254.
- Barnett CT, Brown OH, Bisele M, Brown MJ, De Asha AR, Strutzenberger G. Individuals with Unilateral Transtibial Amputation and Lower Activity Levels Walk More Quickly when Using a Hydraulically Articulating Versus Rigidly Attached Prosthetic Ankle-Foot Device. *JPO: Journal of Prosthetics and Orthotics*. 2018;30(3):158–64.

Patents: US: 7985265, 6719807, 8574312, 8740991, 9132023. EU/RoW: 5336386, 1149568

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